

The University of British Columbia

Department of Electrical and Computer Engineering



Keynote Talk

Visual Quality Enhancement of Low-Dose Dental Cone-Beam Computed Tomography (CBCT) Images

Dr. Simin Mirzaei







Biography





Dr. Simin Mirzaei

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Research interests are primarily in the area of intelligent digital media, visual information capture and delivery, artificial intelligence in digital media with focus on entertainment, security, autonomous driving, smart cities and health.

Active member of the Standards Council of Canada (SCC), MPEG, JPEG







Outline



- 1) Introduction
 - 2 Challenges, Existing Approaches & Limitations
 - 3 Proposed Methods
 - 4 Conclusion
- **5**) Future Work









Introduction



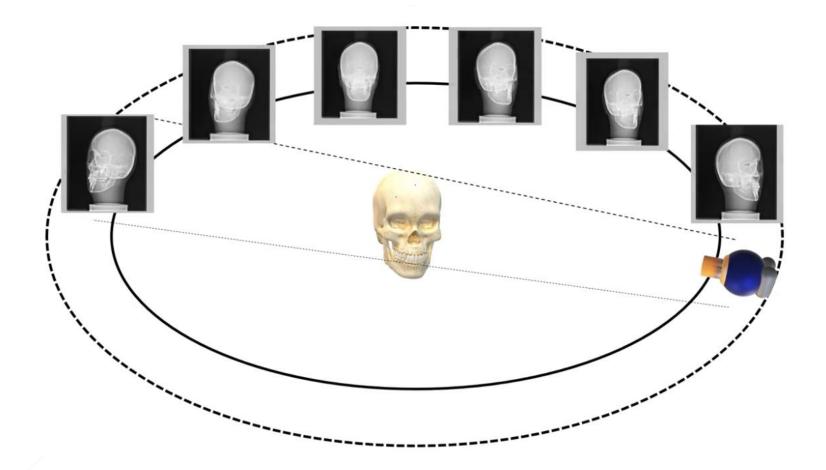




Introduction to CBCT Technology



• CBCT: An advanced imaging technique in dentistry and other medical applications





CBCT imaging device



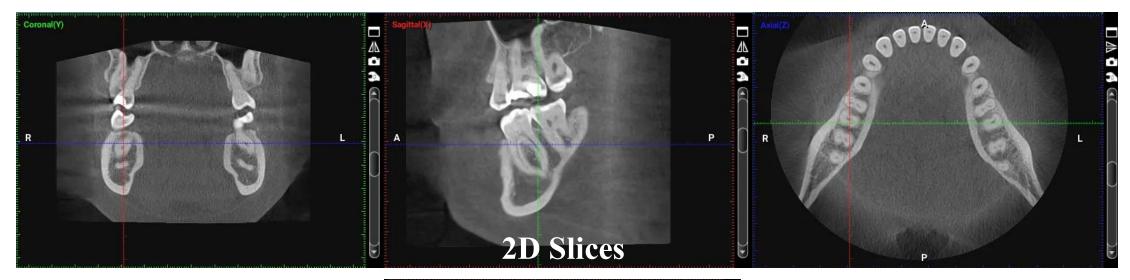


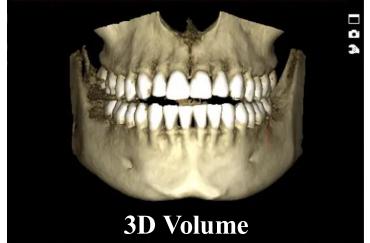


Introduction to CBCT Technology



• CBCT: An advanced imaging technique in dentistry and other medical applications







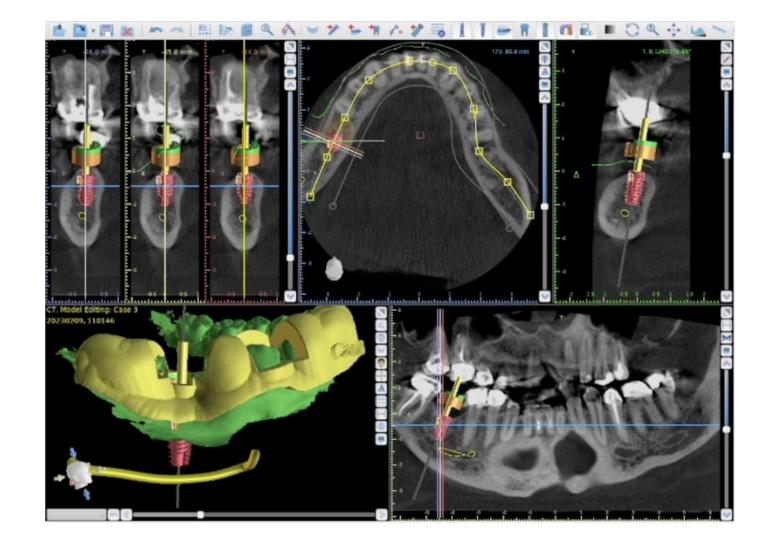




Introduction to CBCT Technology



• Implant placement and surgery planning using CBCT images











Challenges, Existing Solutions and Limitations

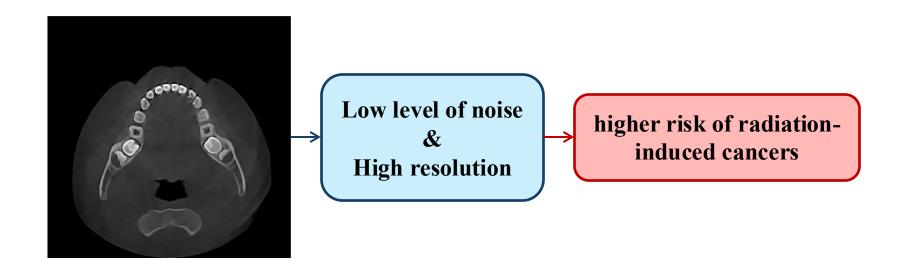








Best image quality possible with high-dose radiation exposure



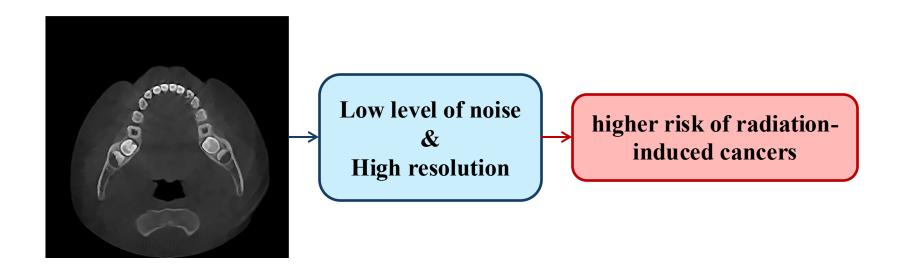




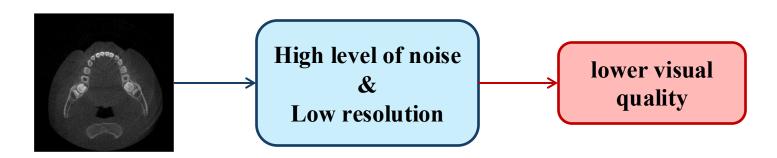




Best image quality possible with high-dose radiation exposure



Industry Solution: Lower the radiation exposure for patient safety







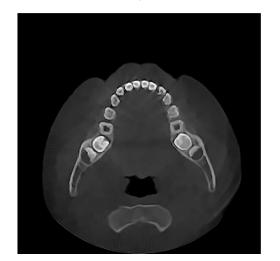


Ideal Solution?



Continue using low radiation exposure for patient safety





Enhance the quality of the CBCT image to match or surpass that of high-dose radiation

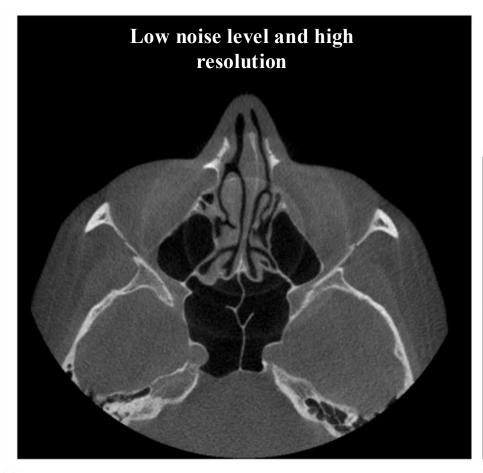


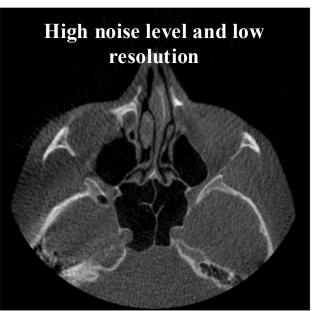






High Noise Levels and Low Resolution







High-dose CBCT image

Low-dose CBCT image





High Noise Levels and Artifacts



Examples of low-dose CBCT images

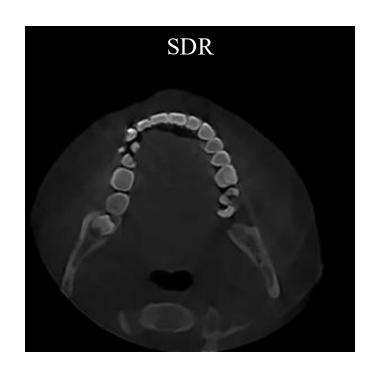


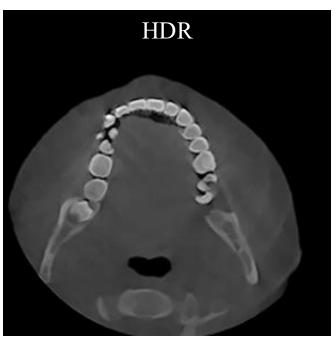






Low Brightness and Contrast – Standard Dynamic Range for CBCT (& Medical) Imaging













Existing Approaches





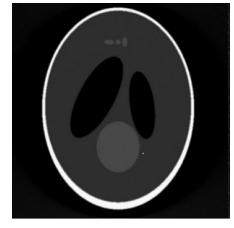




Existing Work on Noise Reduction – Signal Processing based



Not a real CBCT image



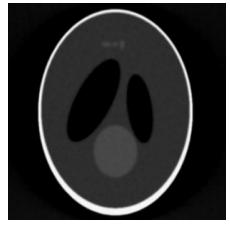
Original



They add fake noise to generate low-dose like CBCT image



Noisy image



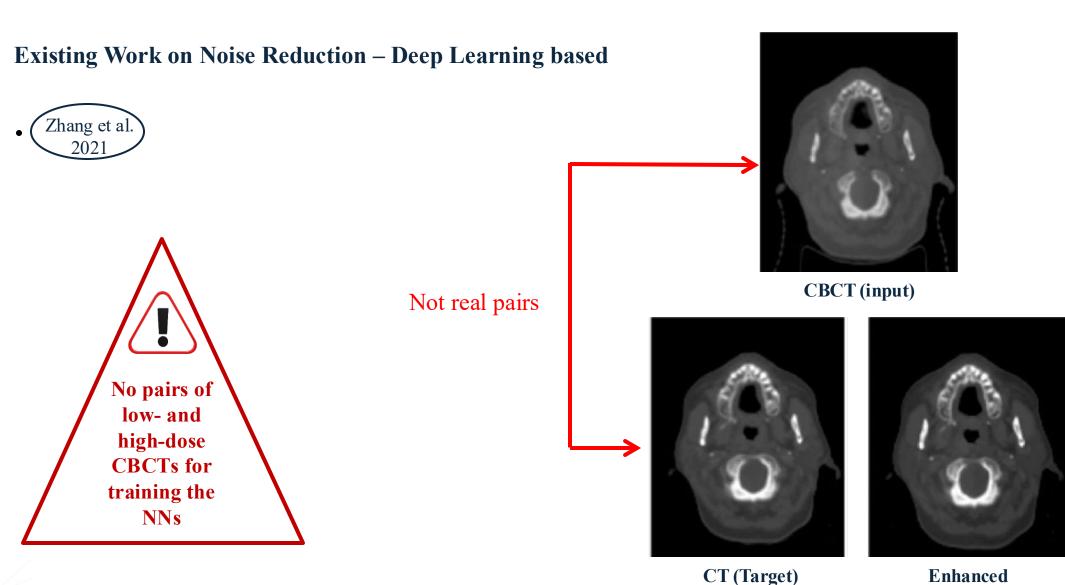
Enhanced











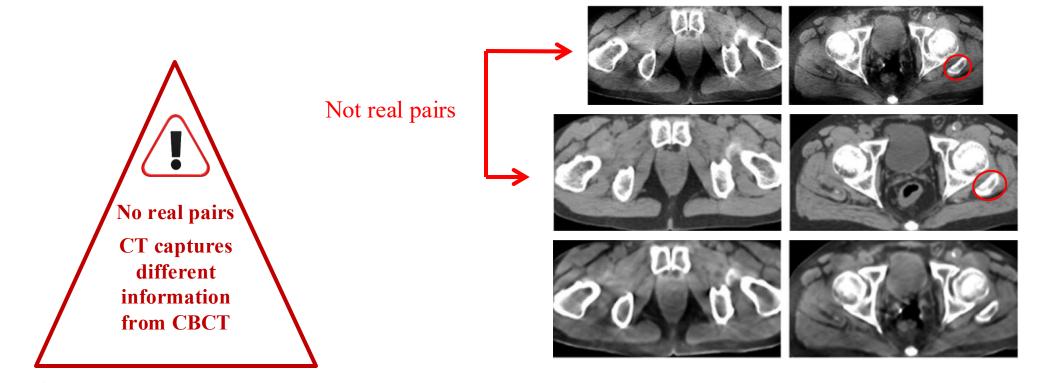






Existing Work on Spatial Resolution Enhancement – Deep Learning based





Low-dose CBCT

Target CT

Enhanced CBCT

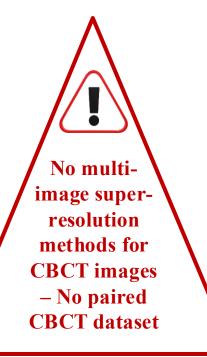




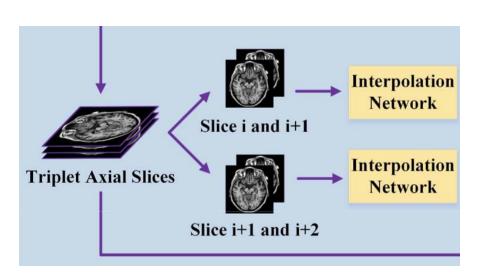


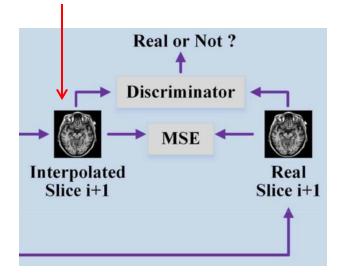
Existing Work on Spatial Resolution Enhancement (for MRI) – Deep Learning based





Use multi-images i, i+1 & i+2 to upscale i+1





Not real pairs
MRI does generalize to CBCT images





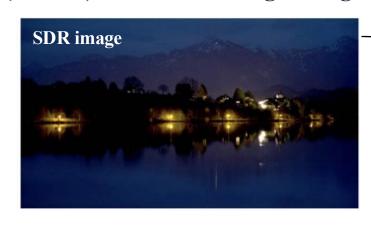


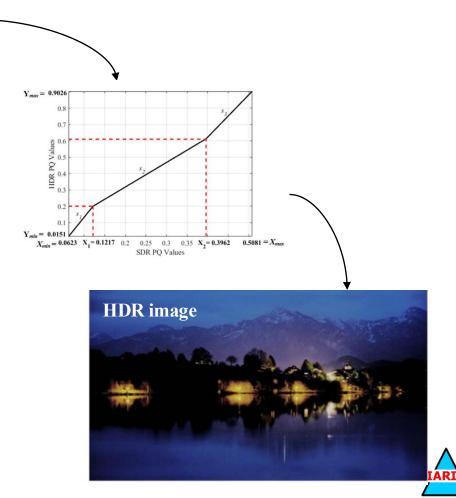
Existing Work on Contrast and Brightness Enhancement of CBCT images

inverse Tone Mapping Operators (iTMOs) for Natural Images – Signal Processing based

• Mohammadi et al. 2021













Existing Work on Contrast and Brightness Enhancement of CBCT images – do not exist inverse Tone Mapping Operators (iTMOs) for Natural Images – Deep Learning based







SDR image



Target HDR image





Key Steps for Quality Improvement



Reduction of Noise and Artifacts

• Spatial Resolution Enhancement

• Enhancement of Contrast and Brightness (iTMO)









Step 1

"Reduction of Noise and Artifacts"



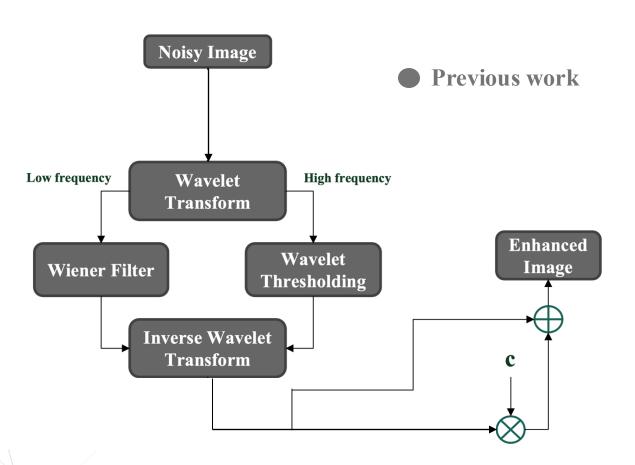






Method 1: Denoising – Assuming Gaussian Noise Distribution

Gaussian noise in low-dose CBCT: y = x + n





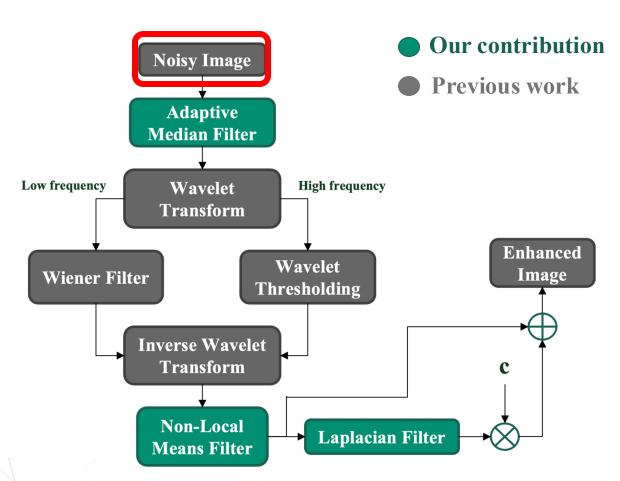






Method 1: Denoising – Assuming Gaussian Noise Distribution

Gaussian noise in low-dose CBCT: y = x + n



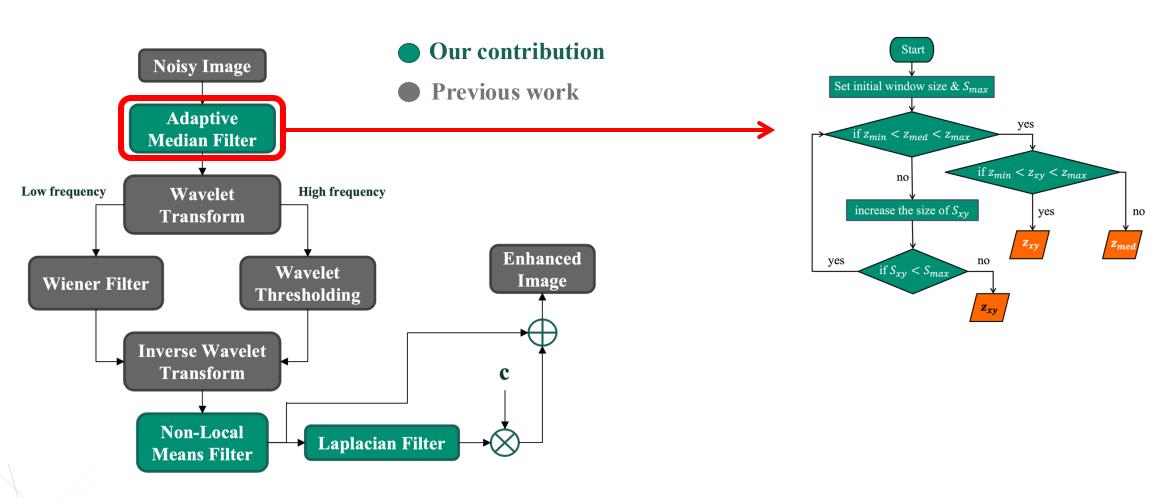






Method 1: Denoising – Assuming Gaussian Noise Distribution

Gaussian noise in low-dose CBCT: y = x + n

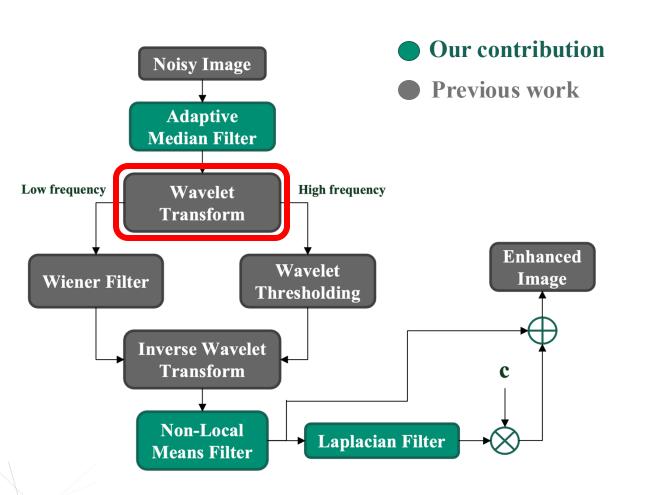


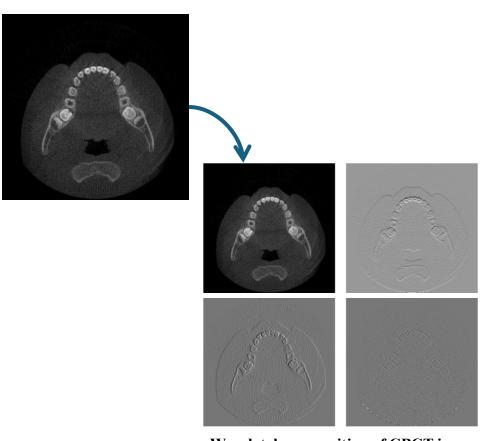


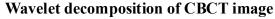








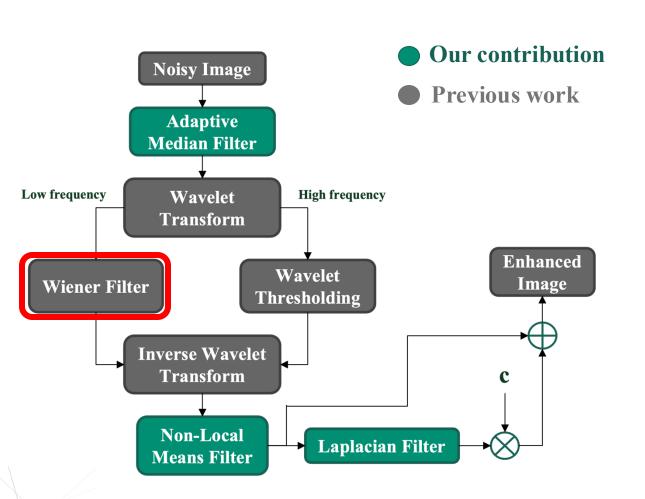












$$I_f(p_i) = \frac{\sigma_l^2}{\sigma_l^2 + v^2} (I_n(p_i) - \mu_l) + \mu_l$$

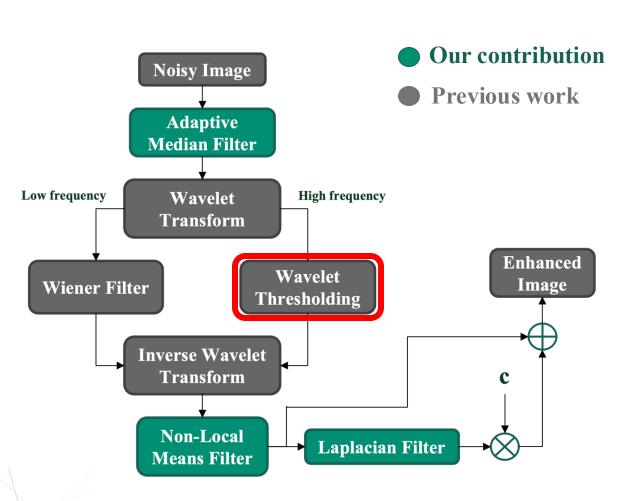
$$v^2 = \frac{Median(cD)}{0.6745}$$







Method 1: Denoising – Assuming Gaussian Noise Distribution



$$w_t = \begin{cases} sign(w)(|w| - T), & |w| \ge T \\ 0, & |w| < 0 \end{cases}$$

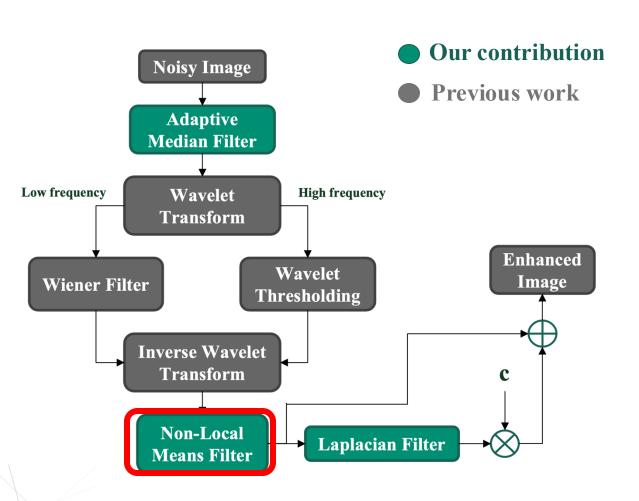
Birge-Massart strategy:

$$\begin{cases} crit(t)_{\min} = \sum c(k)^2 + 2t'\sigma^2 (\alpha + \ln \frac{n}{t'}), k \le t' \\ T = |c(t')| \end{cases}$$

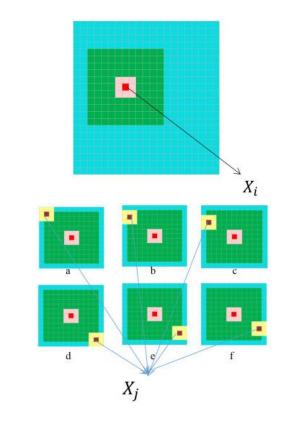








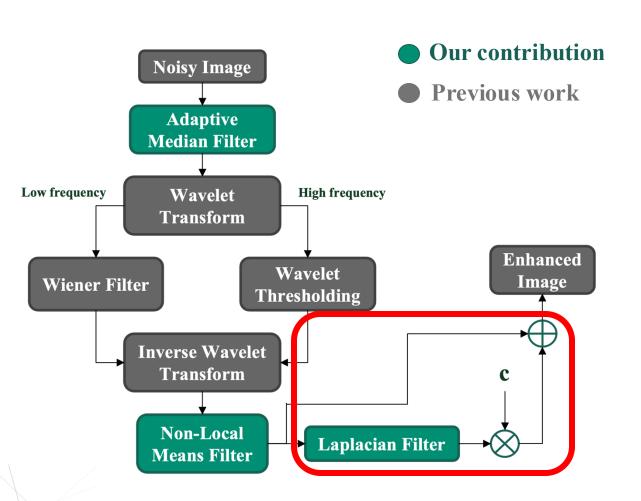
$$I_f(p_1) = \frac{1}{C(p_1)} \sum_{p_2 \in I_n} I_n(p_2) w(p_1, p_2)$$

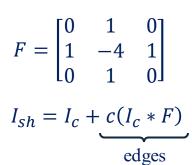


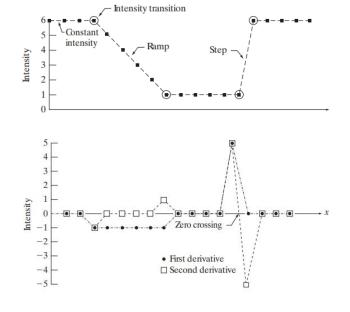










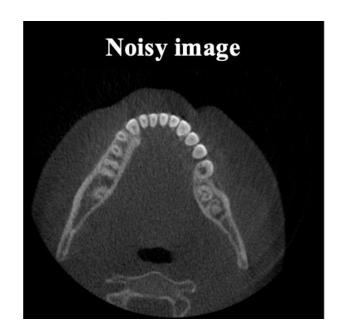




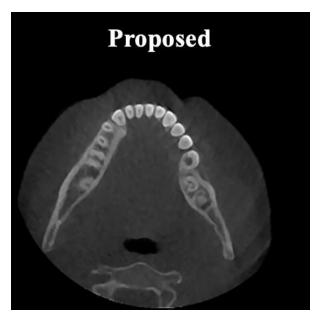




Visual Comparisons









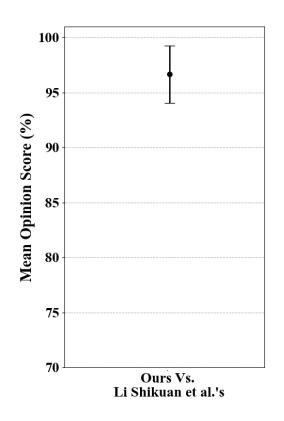




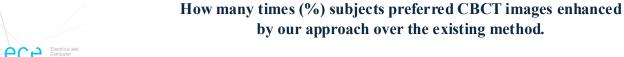


Method 1: Denoising – Assuming Gaussian Noise Distribution

Subjective Evaluations









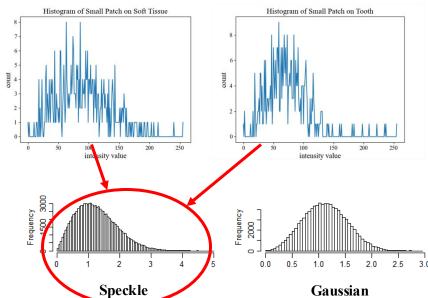




Method 2: Denoising – Assuming Speckle Noise Distribution



Thoroughly analyzed the noise characteristics in CBCT scans captured at various radiation levels and different tissue structures



speckle noise:

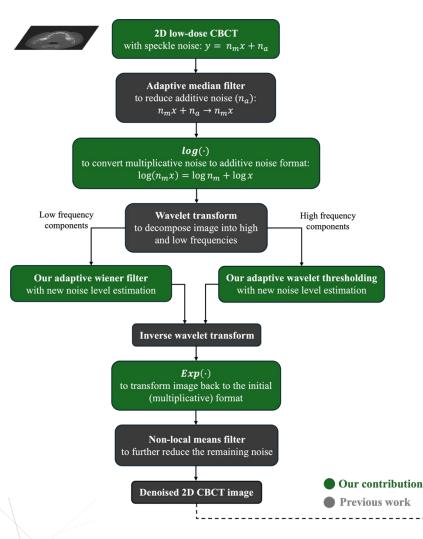
$$y = n_m x + n_a$$

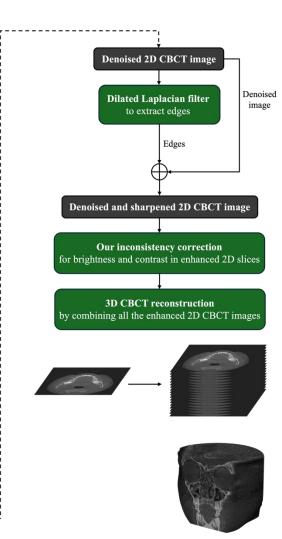






Method 2: Denoising – Assuming Speckle Noise Distribution





Contributions:

- Identifying speckle noise in CBCT images
- Innovative individual filters, and
- An overall filtering framework in which each individual filter is carefully designed and ordered to form a sequence that achieves optimal denoising of CBCT images

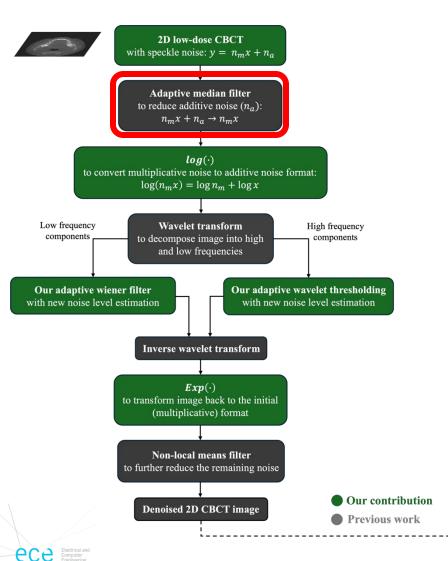


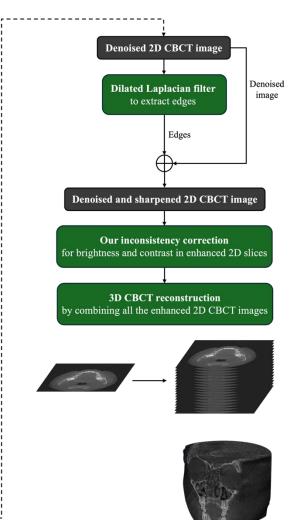


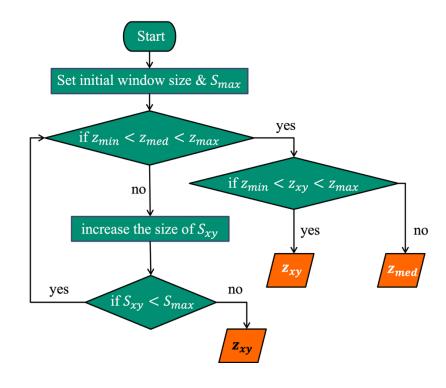




Method 2: Denoising – Assuming Speckle Noise Distribution





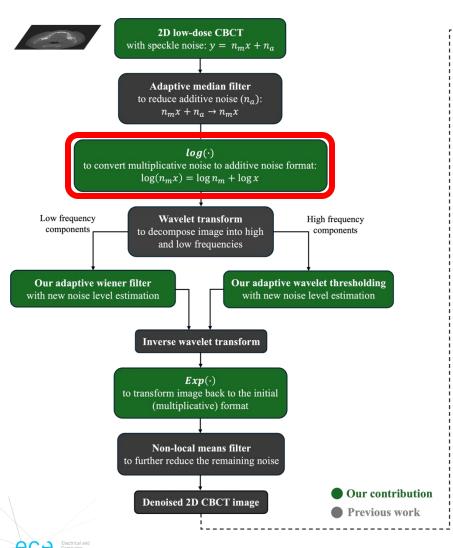


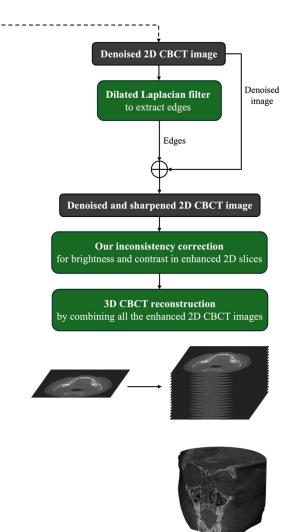






Method 2: Denoising – Assuming Speckle Noise Distribution





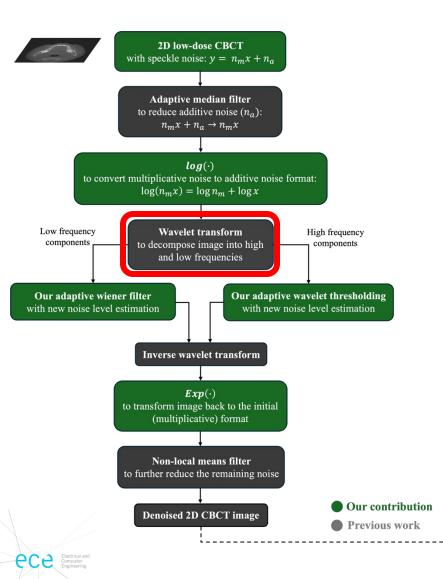
Noisy Image: $y = n_m x + n_a$ Adaptive $y' = n_m x$ median filter: $log y' = log(n_m x) = log n_m + log x$

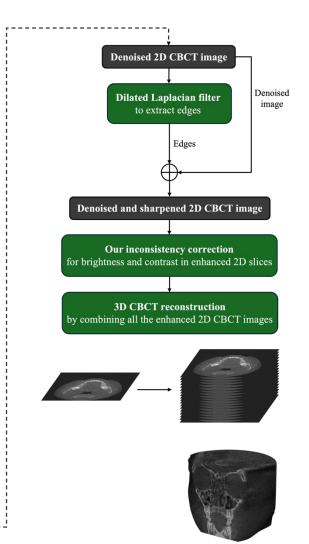
After this step we can use common filters designed for additive noise to remove the multiplicative noise

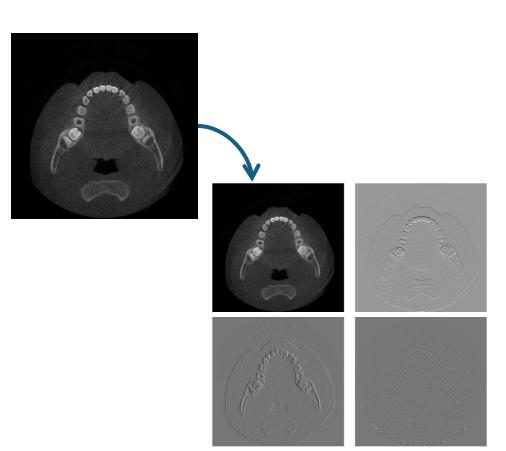










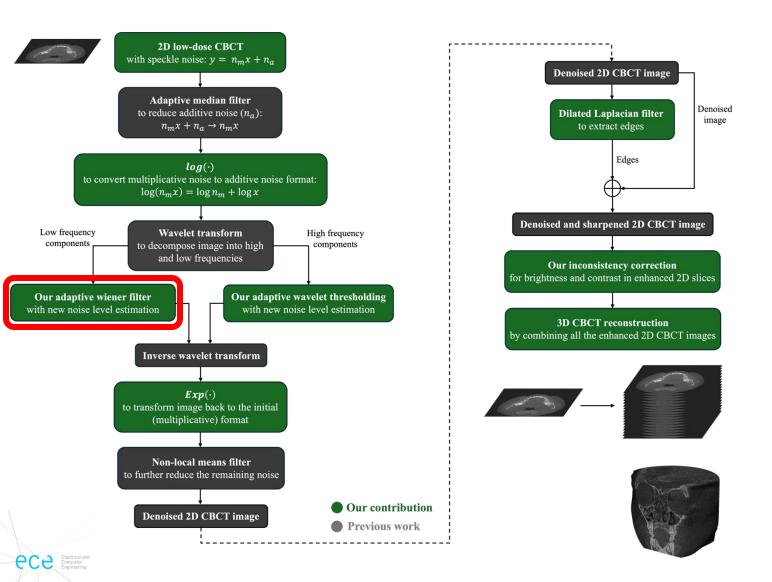


Wavelet decomposition of CBCT image



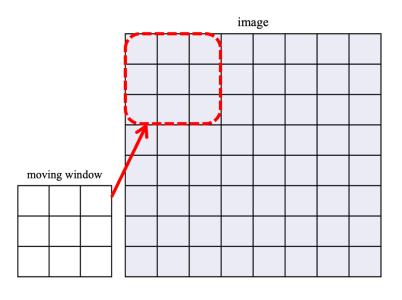






$$I_d = \mu_l + \left(\frac{\max(0, \sigma_l^2 - v^2)}{\max(\sigma_l^2, v^2)}\right) (I_n - \mu_l)$$

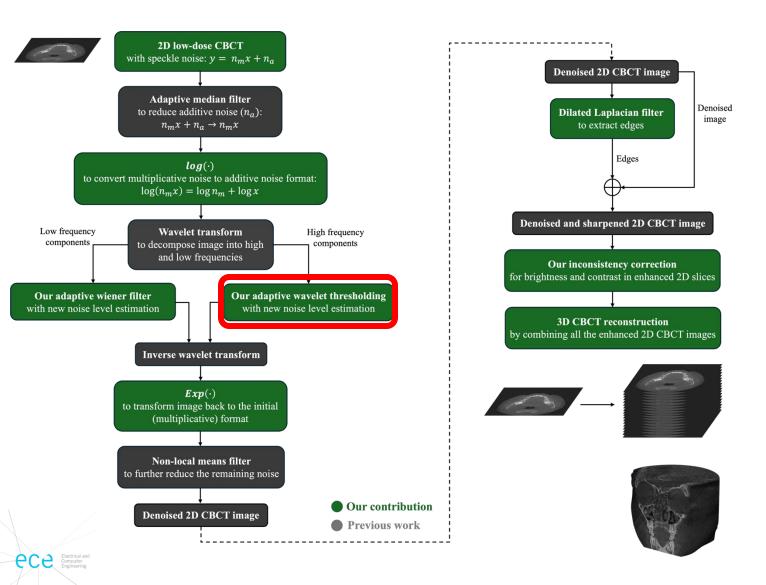
$$v^{2} = \left(\frac{mean(\sigma_{L})}{N}\right) \qquad w = \frac{1}{16} \begin{bmatrix} 0.5 & 1 & 0.5 \\ 1 & 10 & 1 \\ 0.5 & 1 & 0.5 \end{bmatrix}$$







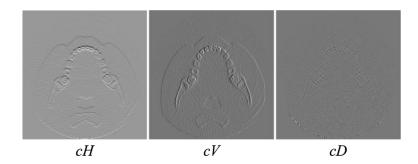




$$v_H^2 = \left(\frac{median(|H|)\sqrt{mean(\sigma_L)}}{N/M}\right)^2$$

$$T = \frac{v_H^2}{\sigma_\chi}$$

$$\sigma_x = \sqrt{max(\sigma_y^2 - v_H^2, \mathbf{0})}$$

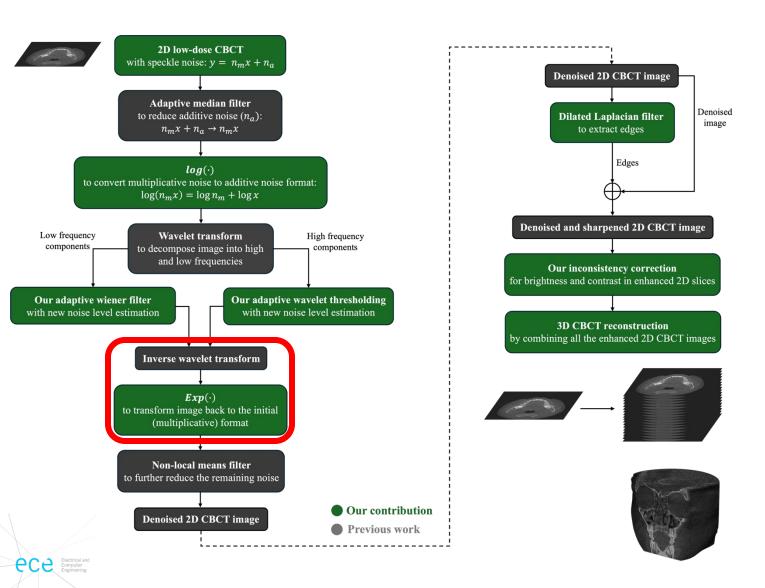








Method 2: Denoising – Assuming Speckle Noise Distribution

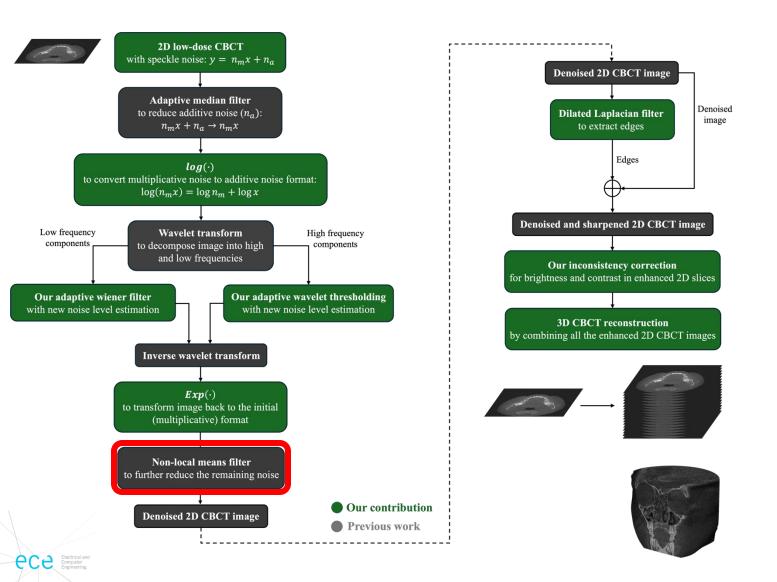


Transfer the image to both spatial and multiplicative noise domain

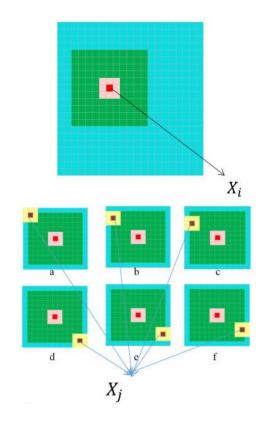








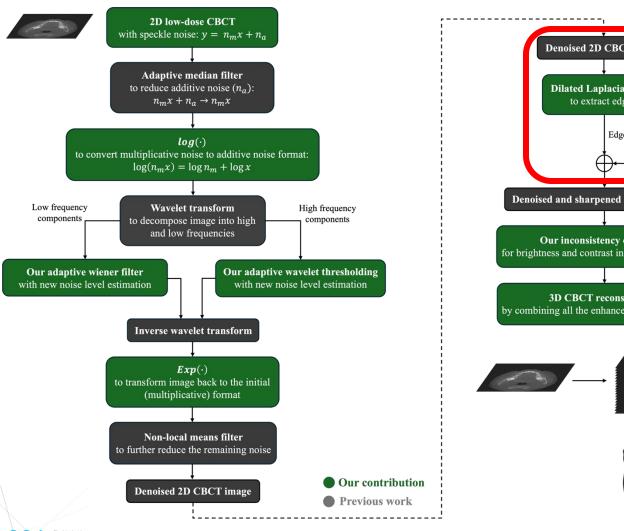
$$I_f(p_1) = \frac{1}{C(p_1)} \sum_{p_2 \in I_n} I_n(p_2) w(p_1, p_2)$$

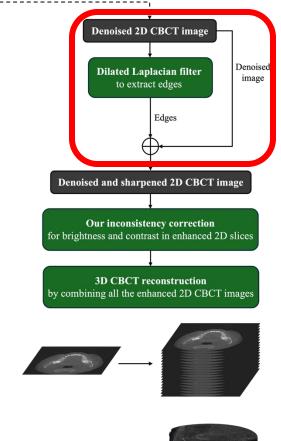




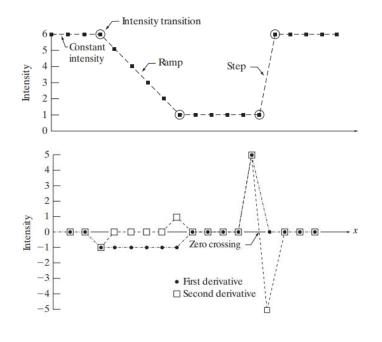








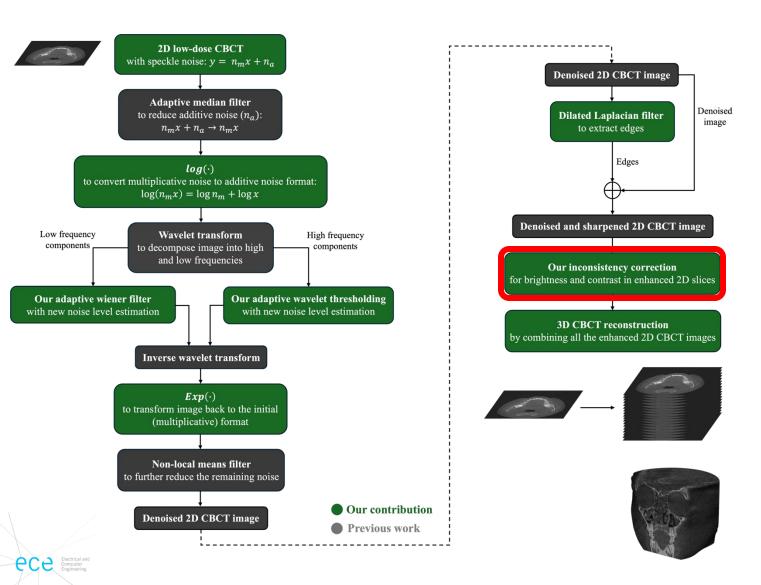
$$F = \begin{bmatrix} 0 & 0 & 1 & 0 & 0 \\ 0 & 0 & 0 & 0 & 0 \\ 1 & 0 & -4 & 0 & 1 \\ 0 & 0 & 0 & 0 & 0 \\ 0 & 0 & 1 & 0 & 0 \end{bmatrix} \qquad I_{sh} = I_c + \underbrace{c(I_c * F)}_{\text{edges}}$$







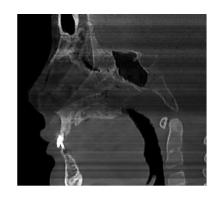




$$r = \frac{mean(I_n - \min(I_n))}{mean(I_f - \min(I_n))}$$

$$I_{n'} = I_n - \min(I_n)$$
$$I_{f'} = I_f - \min(I_n)$$

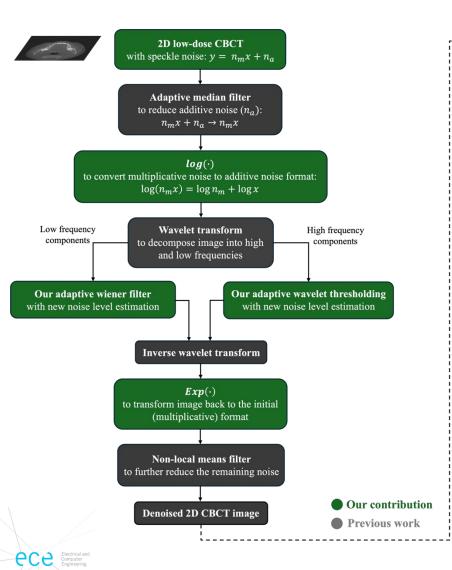
$$\begin{split} I_{out} &= \min(\max(rI_{c'}, \min(I_{n'})), \max(I_{n'})) \\ &+ \min(I_n) \end{split}$$

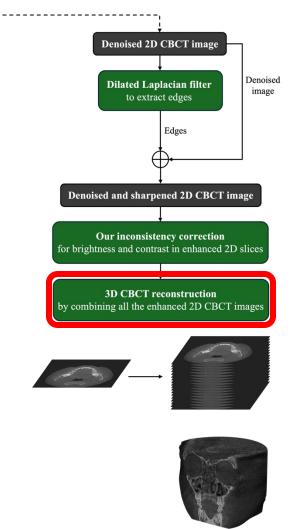


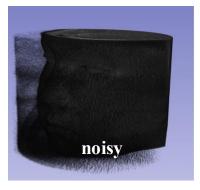


















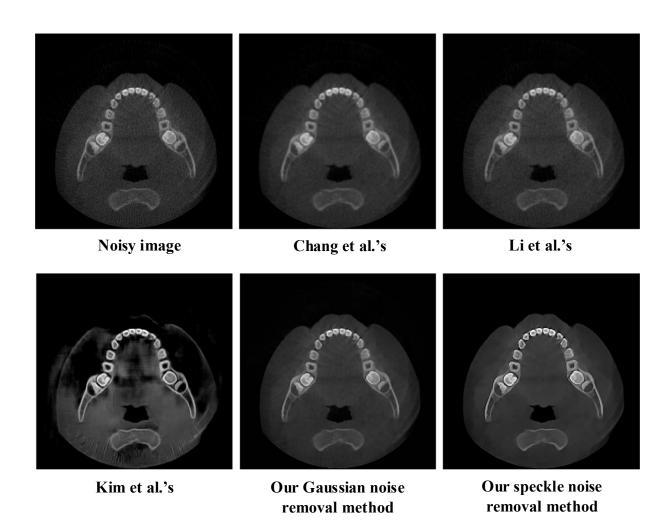






Method 2: Denoising – Assuming Speckle Noise Distribution

Visual comparisons





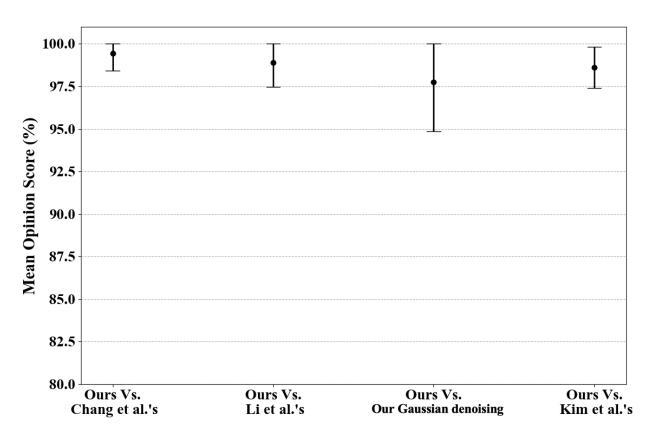






Method 2: Denoising – Assuming Speckle Noise Distribution

Subjective Evaluations



Number of times (%) subjects preferred the visual quality of CBCT images generated by our speckle method over other methods - Mean Opinion Score (MOS)









Method 2: Denoising – Assuming Speckle Noise Distribution

No-Reference Objective Evaluations

BRISQUE and NIQE scores for our method and existing approaches

Techniques	BRISQUE Score	NIQE Score
Noisy Image	50.57	6.14
Chang et al.'s	48.41	5.38
Li et al.'s	48.67	5.65
Mirzaei et al.'s	47.89	4.86
Kim et al.'s	46.24	4.67
Our Method	44.88	3.89

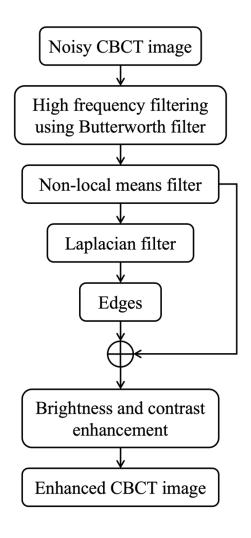








Method 3: Antialiasing Using Frequency and Spatial Domain Filtering



Our Contribution

A filtering framework designed to form a sequence of filtering steps that achieves optimal antialiasing of CBCT images



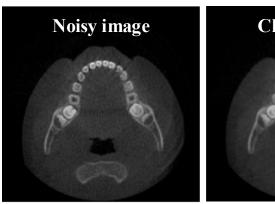


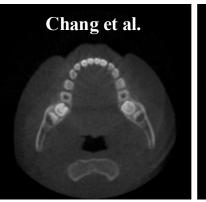




Method 3: Antialiasing Using Frequency and Spatial Domain Filtering

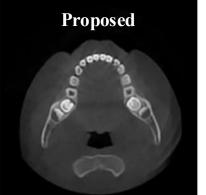
Visual Comparisons













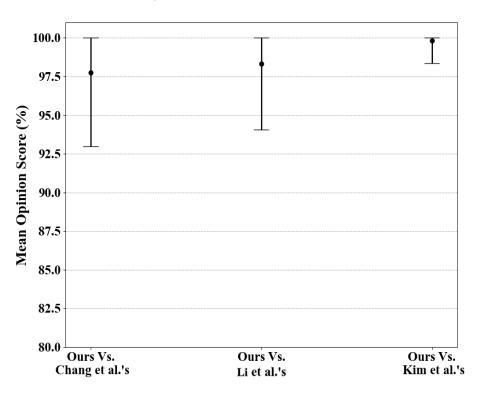






Method 3: Antialiasing Using Frequency and Spatial Domain Filtering

Subjective Evaluations



Number of times (%) subjects preferred the visual quality of CBCT images generated by our approach over other methods - Mean Opinion Score (MOS).

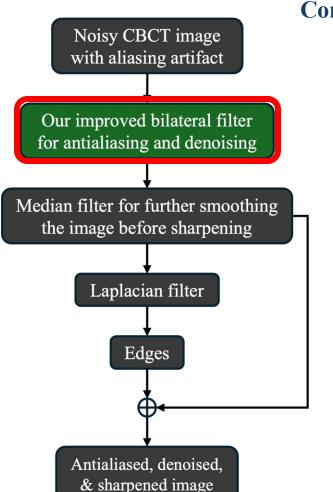








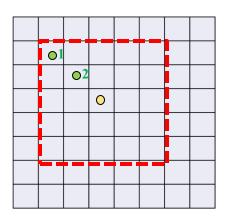
Method 4: Edge-Aware Antialiasing Based on an Enhanced Bilateral Filter



Contribution: Our modified Bilateral filter

Classic Bilateral filter:

$$I_{filtered}(p) = \frac{1}{W_p} \sum_{q \in \Omega} I(q) \cdot exp\left(-\frac{\|p - q\|^2}{2\sigma_s^2}\right) \cdot exp\left(-\frac{|I(p) - I(q)|^2}{2\sigma_i^2}\right)$$
spatial closeness intensity similarity



Our Modified Bilateral Filter:

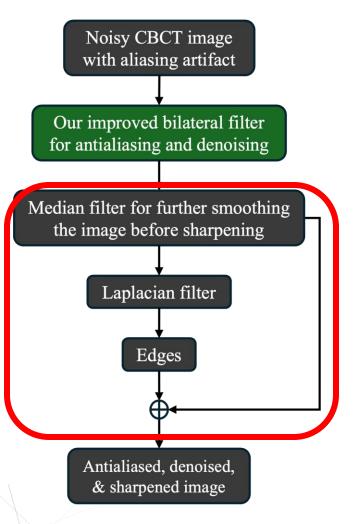
$$I_{filtered}(p) = \frac{1}{W_p} \sum_{q \in \Omega} I(q) \cdot exp\left(-\frac{\|p-q\|^2}{2\sigma_s^2}\right) \cdot exp\left(-\frac{|I(p)-I(q)|^2}{2\sigma_i^2}\right) \cdot exp\left(-\frac{(\|\nabla I(p)\|-\|\nabla I(q)\|)^2}{2\sigma_g^2}\right) \cdot exp\left(-\frac{(std(N_p)-std(N_q))^2}{2\sigma_t^2}\right)$$
spatial closeness intensity similarity
gradient similarity
texture similarity



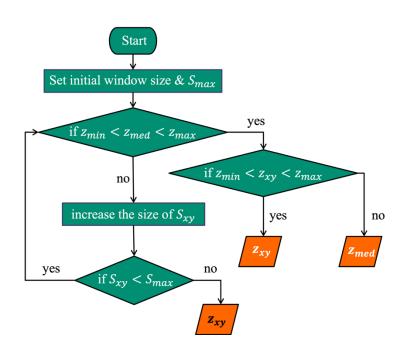




Method 4: Edge-Aware Antialiasing Based on an Enhanced Bilateral Filter



Adaptive Median Filter:



Sharpening:

$$F = \begin{bmatrix} 0 & 1 & 0 \\ 1 & -4 & 1 \\ 0 & 1 & 0 \end{bmatrix}$$

$$I_{sh} = I_c + \underbrace{c(I_c * F)}_{\text{edges}}$$



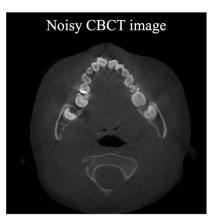






Method 4: Edge-Aware Antialiasing Based on an Enhanced Bilateral Filter

Visual Comparisons













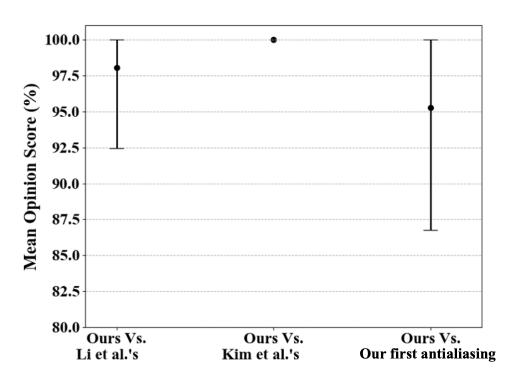






Method 4: Edge-Aware Antialiasing Based on an Enhanced Bilateral Filter

Subjective Evaluations



Number of times (%) subjects preferred the visual quality of CBCT images generated by our approach over other methods - Mean Opinion Score (MOS).



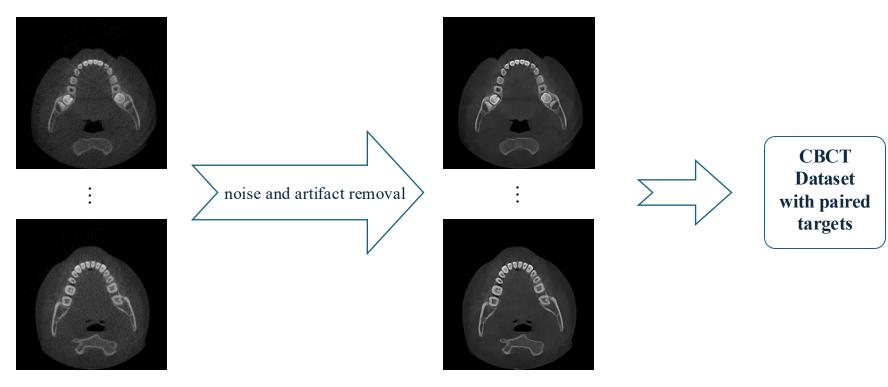






Method 5: Proposed Modified Selective Frequency Network (SFNet) for CBCT Noise Reduction

Contribution: Our unique CBCT dataset





Produced realistic paired targets

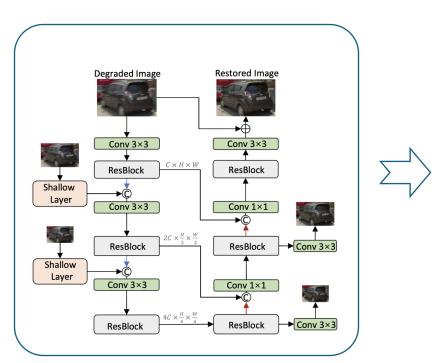




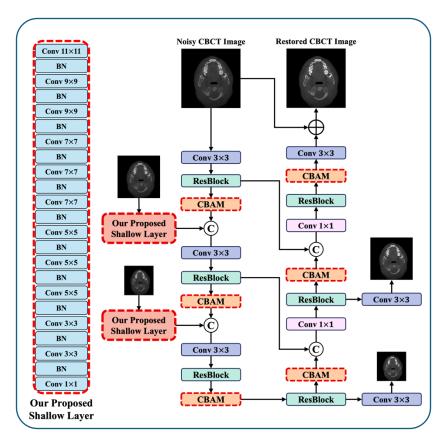




Method 5: Proposed Modified Selective Frequency Network (SFNet) for CBCT Noise Reduction



Original SFNet proposed by Cui et al.



Our improved SFNet







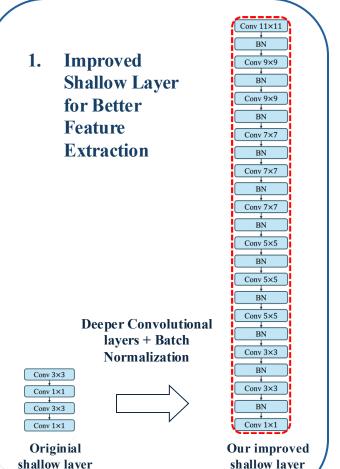
shallow laver

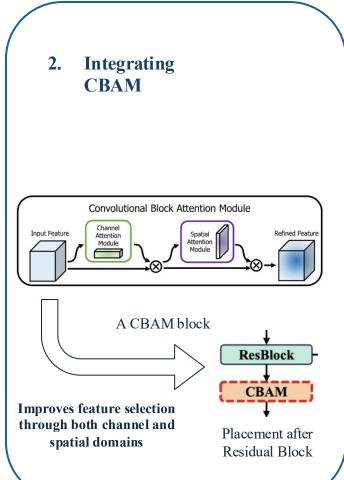
Noise and Artifacts Reduction

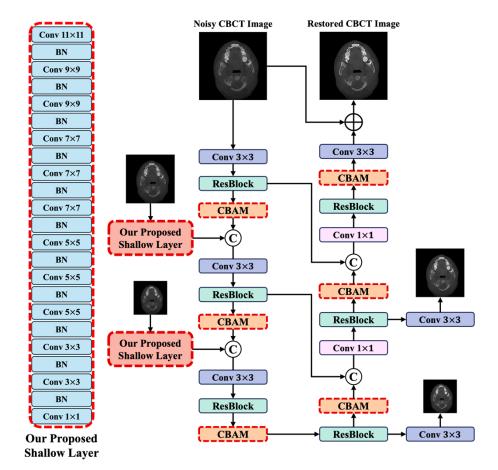


Method 5: Proposed Modified Selective Frequency Network (SFNet) for CBCT Noise Reduction

Contributions: Modifications 1 & 2 to SFNet for optimal denoising of CBCT images







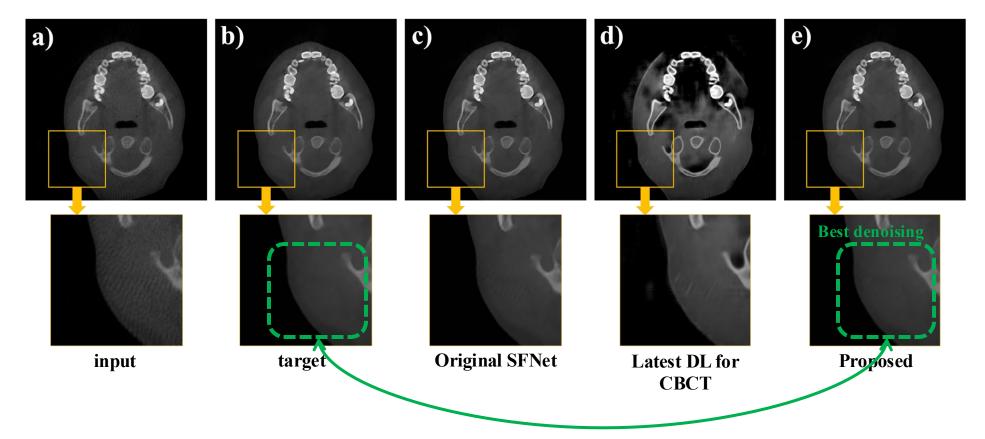






Method 5: Proposed Modified Selective Frequency Network (SFNet) for CBCT Noise Reduction

Visual Comparisons











Method 5: Proposed Modified Selective Frequency Network (SFNet) for CBCT Noise Reduction

Objective Evaluations

Full-Reference Objective Evaluations:

Madhada	Full-Reference		
Methods	PSNR (dB)	MS-SSIM	· _
Original SFNet	44.73	0.9845	
The latest DL method	21.21	0.8101	•
Our modified SFNet	46.77	0.9857	BEST

No-Reference Objective Evaluations:

Images	No-Reference Quality Metric SSEQ
Noisy CBCT image	2.99
Target (generated by us)	2.14
Original SFNet	2.24
The latest DL method	2.51
Our modified SFNet	2.10





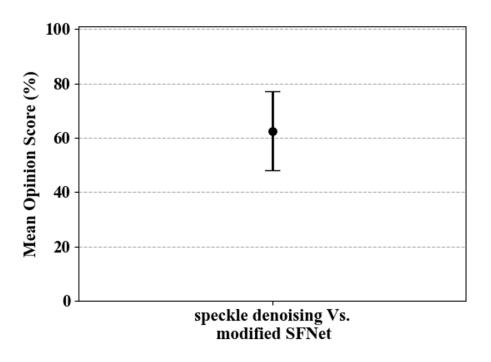






Method 5: Proposed Modified Selective Frequency Network (SFNet) for CBCT Noise Reduction

Subjective Evaluations



Best Denoising: our speckle noise reduction method









Step 2

"Spatial Resolution Enhancement"



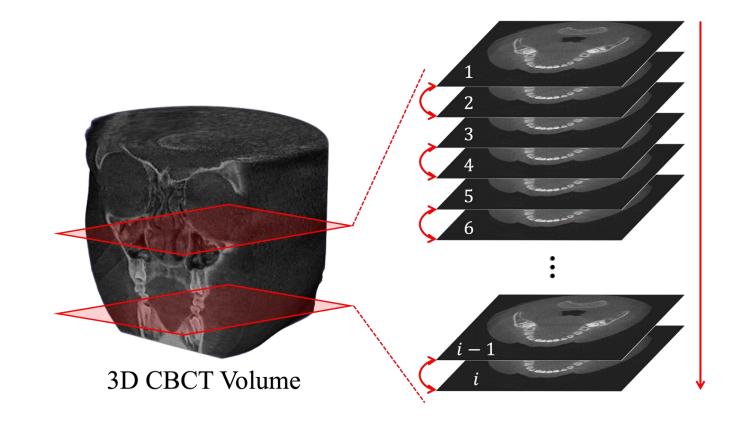






Proposed Lightweight StereoMamba for CBCT Resolution Enhancement

Contribution: Leveraging information between adjacent CBCT scans to upscale both scans











Proposed Lightweight StereoMamba for CBCT Resolution Enhancement

Results of our comparative analysis of existing Single-Image Super-Resolution (SISR) & Stereo-Image Super-Resolution (SSR) methods

	Method	#S	#Params	PSNR	SSIM
SISR {	SwinIR	x2	11.28M	36.32	0.9849
	NAFSSR-T	x2	0.45M	36.72	0.9865
	NAFSSR-S	x2	1.54M	36.65	0.9859
SSR	NAFSSR-B	x2	6.77M	36.47	0.9857
	NAFSSR-L	x2	23.79M	36.08	0.9846
	StereoMamba	x2	7.55M	35.88	0.9840



Large, complex models tend to overfit when applied to content with much lower complexity

➤ The most promising architecture But worst generalizability



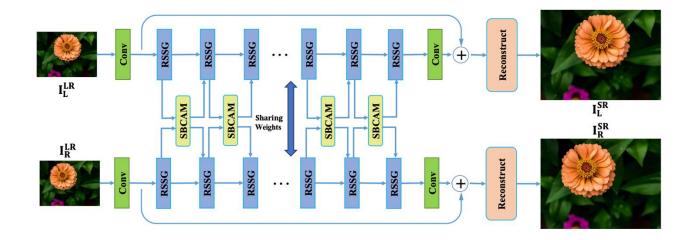






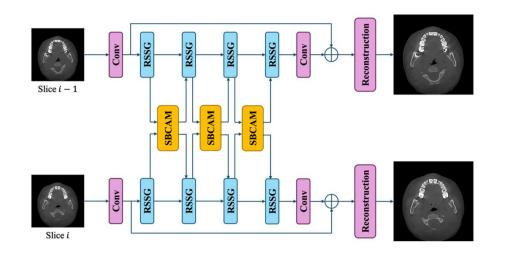
Proposed Lightweight StereoMamba for CBCT Resolution Enhancement

Original StereoMamba:



Contribution: Modifying StereoMamba to optimize upscaling of CBCT images

StereoMamba-Light:



A lightweight version without memorizing dataset-specific details









Proposed Lightweight StereoMamba for CBCT Resolution Enhancement

No-Reference Objective Evaluations

NIQE scores for our method and existing approaches

SISR {	Method	#S	#Params	NIQE
	SwinIR	x2	11.28M	5.1
SSR	NAFSSR-T	x2	0.45M	4.2
	NAFSSR-S	x2	1.54M	4.5
	NAFSSR-B	x2	6.77M	4.8
	NAFSSR-L	x2	23.79M	5.4
	StereoMamba	x2	7.55M	6.1
	StereoMamba-Light	x2	0.9M	3.7









Step 3

"Brightness and Contrast Enhancement"







Brightness and Contrast Enhancement



inverse Tone Mapping Operator (iTMO)

SDR Image HDR Image









Conclusion

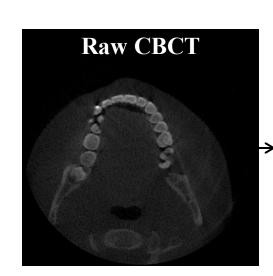




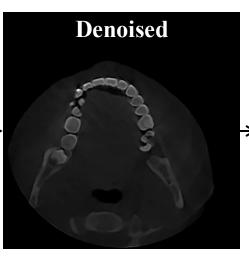


Conclusion

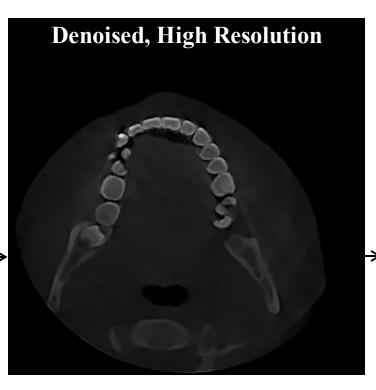




Noisy, Low Resolution, SDR CBCT Image



Denoising



Super Resolution



Inverse Tone Mapping









Thank you



